

# Control engineering challenges and results

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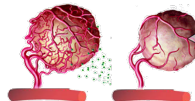
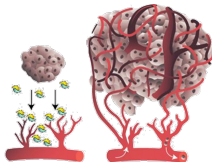
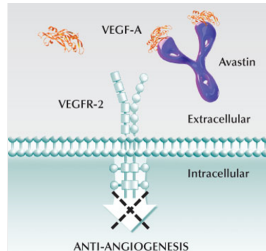
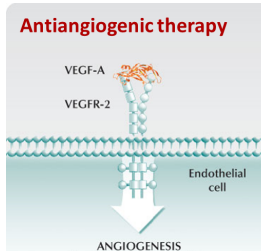
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# Antiangiogenic therapy





# Hahnfeldt model (1999)<sup>1</sup>

$$\begin{aligned}\dot{x}_1 &= -\lambda_1 x_1 \ln \left( \frac{x_1}{x_2} \right) \\ \dot{x}_2 &= bx_1 - dx_1^{2/3} x_2 - ex_2 u\end{aligned}$$

- $x_1$  is the function of tumor volume
- $x_2$  is the function of endothelial volume (blood vessels)
- $u$  is the function of inhibitor level in the patient

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<sup>1</sup>P. Hahnfeldt et al., Tumor Development under Angiogenic Signaling: A Dynamical Theory of Tumor Growth, Treatment Response, and Postvascular Dormancy, Cancer Research 59, pp. 4770–4775, 1999

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## The minimal model – Differential equation

Linear dynamics expanded with bilinear term:

$$\dot{x}(t) = ax(t) - bx(t)y(t) = (a - by(t))x(t)$$

- $x$  is the function of tumor volume ( $\text{mm}^3$ )
- $y$  is the inhibitor level in the patient ( $\text{mg/kg}$ )
- $a$  is the tumor growth rate ( $1/\text{day}$ )
- $b$  is the inhibition rate ( $\text{kg}/(\text{mg} \cdot \text{day})$ ).

The pharmacokinetics of the inhibitor is linear, i.e.

$$\dot{y}(t) = -cy(t) + I(t)$$

- $u$  is the function of inhibitor injection rate ( $\text{mg}/(\text{kg} \cdot \text{day})$ )
- $c$  is the clearance of the inhibitor ( $1/\text{day}$ ).

# LS estimation

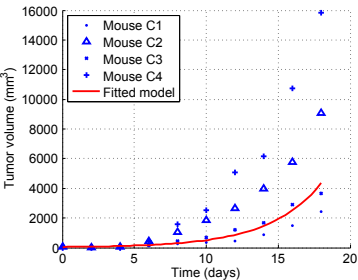
The values of the identified parameters are

- $x(0) = 45.46 \text{ mm}^3$ ;
- $a = 0.27 \text{ 1/day}$ ;
- $b = 0.0074 \text{ kg/ (mg} \cdot \text{day)}$ .

$$x(t) = 45.46 \exp(0.27t - \dots)$$

Results without therapy  
from 2014<sup>3</sup>

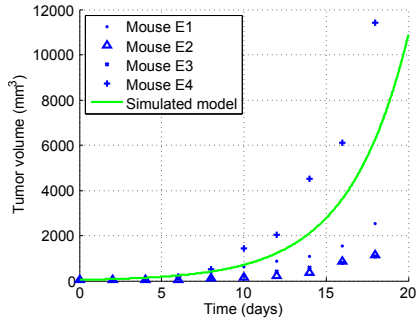
$$\begin{aligned} x(t) &= 29020 \exp(0.29788t) \\ &\quad - 29010 \exp(0.29789t) \\ &\approx 10 \exp(0.29789t) \end{aligned}$$



<sup>c</sup>J. Sápi et al., CINTI 2014, pp. 443–448

# Validation

Mice got injection each day, simulation is carried out with parameters acquired from identification.



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# Motivation and control problem

- The control input in most physiological systems is nonnegative.
- Most controllers can not ensure that the input is positive without using saturation.
- Saturation distorts the model and may lead to unexpected behavior.
- Moreover, physiological models are usually nonlinear.

## Ensuring positive input

$$\begin{aligned}\dot{x}(t) &= ax(t) - bx(t)y(t) \\ \dot{y}(t) &= -cy(t) + I(t)\end{aligned}$$

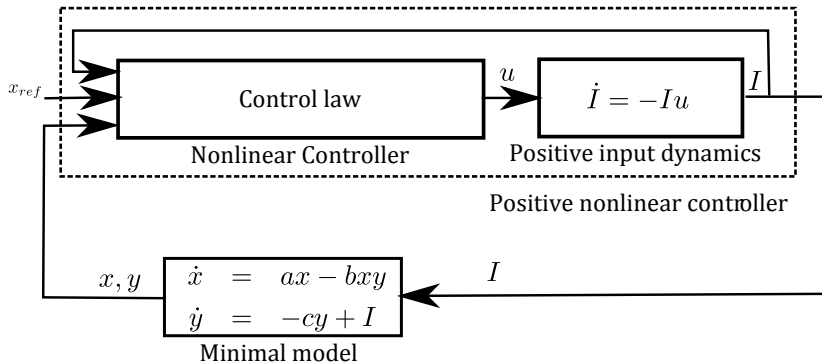
Denote the rate of injection (input of the physiological system) by  $I$ , and introduce the fictive input dynamics

$$\dot{I}(t) = -I(t)u(t)$$

and let  $u$  be the new (fictive) input. The new differential equation ensures that  $I(t)$  is positive for all  $t > 0$  if  $I(0) > 0$ . The fictive input  $u$  can be negative.



## Ensuring positive input



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# Path tracking control

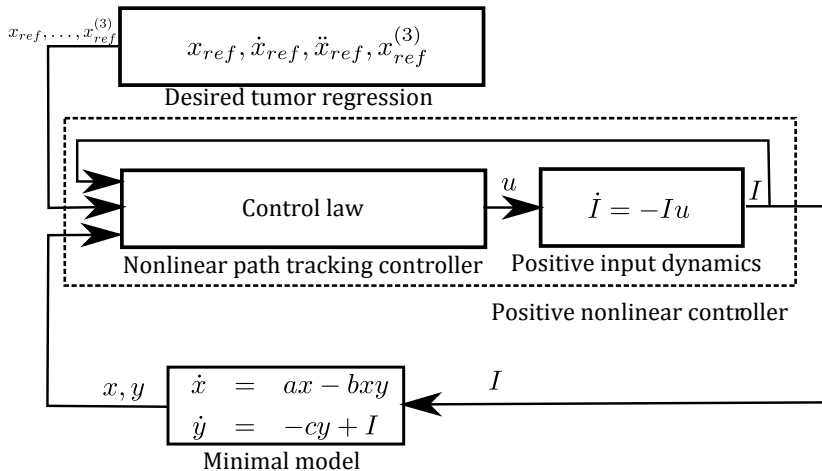
We apply the control law

$$u = \frac{k_0(x_{ref} - h) + k_1(\dot{x}_{ref} - L_f h) + k_2(\ddot{x}_{ref} - L_f^2 h) + x_{ref}^{(3)} - L_f^3 h}{b x l}.$$

with

$$\begin{aligned} h &= x \\ f &= \begin{pmatrix} ax - bxy \\ -cy + I \\ 0 \end{pmatrix} \\ L_f h &= h' f \\ L_f^2 h &= (L_f h)' f \\ L_f^3 h &= (L_f^2 h)' f \end{aligned}$$

# Path tracking control



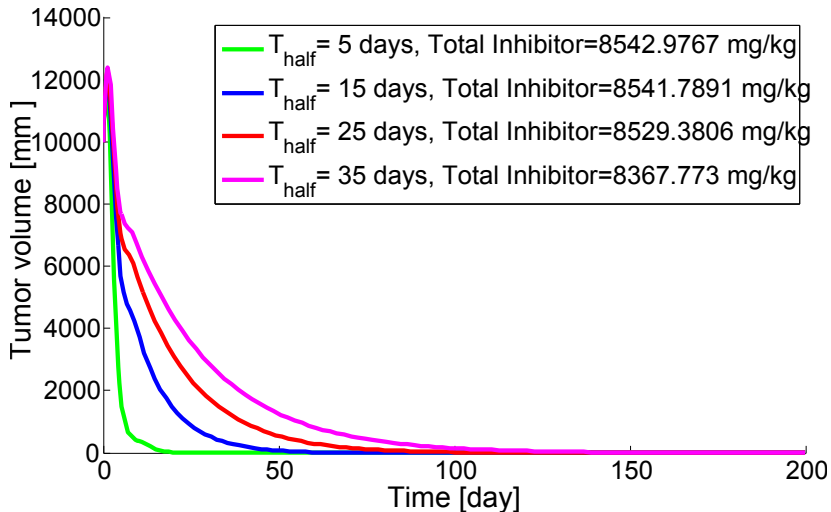
# Results

The reference tumor volume in our simulations is

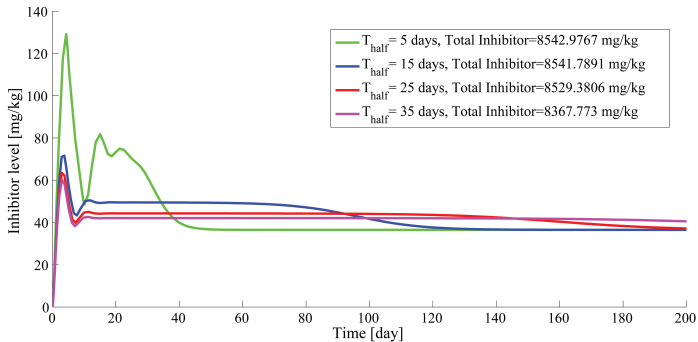
$$x_{ref} = (x(0) - 1)e^{-t/(\ln(2)T_{half})}$$

and its derivatives. We analyze the results acquired with different  $T_{half}$  half-times.

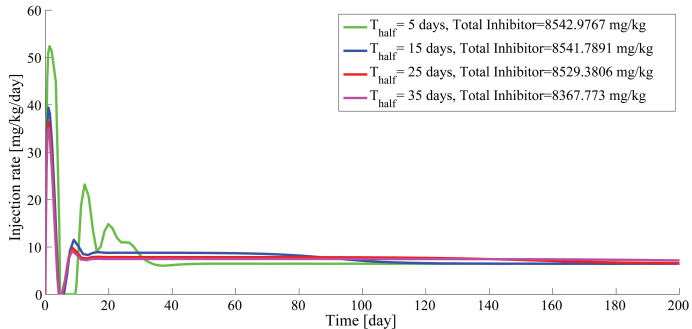
# Tumor volume



# Inhibitor level



# Injection rates





# Thank you for your attention!

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